

C. Remarks

This Preliminary Amendment is to submit a substitute specification to correct various typographical, grammatical and syntax errors to conform the text better with proper idiomatic English. Also, it includes the change made in the Preliminary Amendment filed on July 9, 2004. A copy of the original specification, showing the changes made thereto, is attached.

No new matter has been added. Favorable consideration of the claims and expedient passage to issue are respectfully requested.

Applicants' undersigned attorney may be reached in our New York office by telephone at (212) 218-2100. All correspondence should continue to be directed to our below listed address.

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BIOCHEMICAL REACTION CARTRIDGE

FIELD OF THE INVENTION AND RELATED ART

The present invention relates to a biochemical  
5 reaction cartridge ~~used to~~ that can be incorporated in  
an apparatus for analyzing a cell, a microorganism, a  
chromosome, a nucleic acid, etc., in a specimen by  
utilizing a biochemical reaction, such as  
antigen-antibody reaction, or nucleic acid  
10 hybridization.

Most ~~of~~ analyzers for analyzing specimens, such  
as blood, uses an immunological procedure utilizing an  
antigen-antibody reaction or a procedure utilizing  
nucleic acid hybridization. For example, protein or  
15 single-stranded nucleic acid, such as antibody or  
antigen, which specifically ~~connects~~ hybridizes with a  
material or substance to be detected, is used as a  
probe and is fixed on a surface of a solid phase, such  
as fine particles, beads or a glass plate, thus  
20 effecting the antigen-antibody reaction or nucleic  
acid hybridization. Then, for example, an  
antigen-antibody compound or double-stranded nucleic  
acid is detected by a labeled antigen or labeled  
nucleic acid, which causes a specific interaction,  
25 such that a labeled material having a high detection  
sensitivity, such as an enzyme, a fluorescent material  
or a luminescent material, is supported, thus

effecting detection of presence or absence of the material to be detected or a quantitative determination regarding the detected material.

As an extension of these technologies, e.g., U.S.  
5 Patent No. 5,445,934 ~~has disclosed~~ discloses a so-called DNA (deoxyribonucleic acid) array, wherein a large number of DNA probes having mutually different base sequences are arranged on a substrate in an array form.

10 Further, Anal. Biochem., 270(1), pp. 103 - 111 (1999) ~~has disclosed~~ discloses a process for preparing a protein array, like the DNA array, such that various species of proteins are arranged on a membrane filter. By using these DNA and protein arrays and the like, it  
15 has become possible to ~~effect a test on~~ a large number of items at the same time.

Further, in various methods of the specimen analysis, in order to ~~realize alleviation~~ alleviate ~~of the~~ contamination by the specimen, ~~promotion~~ promote  
20 ~~of~~ reaction efficiency, ~~reduction~~ reduce ~~in the~~ size of the ~~apparatus~~ size, and ~~facilitation~~ facilitate ~~of the~~ operation, there have been also proposed disposable biochemical reaction cartridges in which a necessary reaction is performed ~~in the cartridge~~. For  
25 example, Japanese Laid-Open Patent Application (JP-A) (Tokuhyo) Hei 11-509094 ~~has disclosed~~ discloses a biochemical reaction cartridge, including DNA array,

in which a plurality of chambers are disposed and a  
solution is moved by a differential pressure, so as to  
permit a reaction, such as extraction, amplification  
or hybridization of DNA in a specimen, within the  
5 cartridge.

As a method of supplying a reagent with respect  
to the biochemical reaction cartridge, JP-A  
2000-266759 ~~has disclosed~~ discloses that a reagent is  
supplied from an external reagent bottle to a  
10 disposable analysis cassette. Further, JP-A (Tokuhyo)  
Hei 11-5059094 ~~has disclosed~~ discloses that a reagent  
is incorporated in a chamber in advance.

However, in the case of externally supplying the  
reagent, a plurality of reagents must be prepared  
15 separately from the biochemical reaction cartridge,  
and if the number of test items is large, the number  
of necessary reagents is also increased. As a result,  
replenishment of the reagents becomes complicated and  
there is a possibility of erroneously selecting the  
20 species of the reagents. Further, when ~~in the case of~~  
~~incorporating the reagent~~ is incorporated into the  
chamber of the biochemical reaction cartridge, ~~there~~  
~~it is a possibility possible~~ such that a reaction  
different from ~~an~~ that ~~intended reaction is caused~~  
25 ~~to~~ can occur ~~by flowing of~~ if the reagent flows ~~in the~~  
~~chamber~~ into a passage or another chamber due to an  
environmental change at the time of storage or

conveyance, or vibration during conveyance.

#### SUMMARY OF THE INVENTION

An object of the present invention is to provide  
5 a biochemical reaction cartridge, having solved the  
~~above~~ above-described problems, which eliminates the  
inconvenience of replenishment of a reagent and  
erroneous selection of the species of reagent and  
~~causes no flowing of~~ does not cause the reagent in a  
10 chamber to flow into a passage or vibration at the  
time of storage or conveyance.

Another object of the present invention is to  
provide a biochemical reaction apparatus for effecting  
a biochemical reaction by using the biochemical  
15 reaction cartridge.

According to the present invention, there is  
provided a biochemical reaction cartridge, comprising:

a reaction portion, comprising a chamber and a  
passage, for effecting a biochemical reaction, and  
20 a solution storage portion, which is isolated or  
separated from the reaction portion, for storing a  
solution ~~in~~ at a position corresponding to the  
chamber,

wherein the cartridge is provided with a  
25 penetrable partition member disposed between the  
solution storage portion and the reaction portion so  
as to move the solution from the solution storage

portion to the chamber of the reaction portion.

These and other objects, features and advantages  
of the present invention will become more apparent  
upon a consideration of the following description of  
5 the preferred embodiments of the present invention  
taken in conjunction with the accompanying drawings.

#### BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 is a perspective view of an embodiment  
10 of the biochemical reaction cartridge according to the  
present invention.

Figure 2 is a plan view of a solution storage  
portion.

Figure 3 is a partial sectional view of the  
15 biochemical reaction cartridge at the time of storage.

Figure 4 is a partial sectional view of the  
biochemical reaction cartridge in such a state that a  
valve stem (rod) is pressed by first-stage pushing.

Figure 5 is a partial sectional view of the  
20 biochemical reaction cartridge in such a state that a  
valve stem is pressed by second-state pushing.

Figure 6 is a plan view of a reaction portion.

Figure 7 is a block diagram of a treatment  
apparatus for controlling the movement of a solution  
25 and various reactions within the biochemical reaction  
cartridge.

Figures 8A and 8B ~~is~~ show a flow chart of a first

treatment procedure.

~~Figure~~ Figure 9 is a longitudinal sectional view of a part of the chambers shown in Figure 6.

Figure 10 is a longitudinal sectional view of  
5 another part of the chambers shown in Figure 6.

#### DESCRIPTION OF THE PREFERRED EMBODIMENTS

~~Hereinbelow~~ Below, the present invention ~~will be~~ is  
described more specifically with reference to the  
10 drawings.

Figure 1 is a perspective view of a biochemical reaction cartridge in this embodiment. Referring to Figure 1, the cartridge has a two-layer structure including a reaction portion 1, where a reaction is  
15 effected, and a solution storage portion 2 disposed thereon for storing solutions, such as a reagent and a cleaning agent.

A body of each of the reaction portion 1 and the solution storage portion 2 comprises a synthetic  
20 resin, such as polymethyl methacrylate (PMMA), acrylonitrile-butadiene-styrene (ABS) copolymer, polystyrene, polycarbonate, polyester or polyvinyl chloride. In the case where an optical measurement is required, the material for the body of the reaction  
25 portion 1 is required to be a transparent or semitransparent plastic.

At an upper portion of the reaction portion 1, a

specimen port 3 for injecting a specimen, such as  
blood, by a syringe (injector) is disposed and sealed  
up with a rubber cap. On both side surfaces of the  
reaction portion 1, there is a plurality of nozzle  
5 ports 4, into which nozzles are injected to apply or  
reduce pressure in order to move a solution in the  
reaction portion 1. A rubber cap is fixed on each of  
the nozzle ports 4. The other side surface of the  
reaction portion 1 has a similar structure.

10 Further, to an upper portion of the solution  
storage portion 2, 3 aluminum foil sheets are applied  
for blocking an upper portion of a solution storage  
chamber described later. The reaction portion 1 and  
the solution storage portion 2 are bonded to each  
15 other through ultrasonic fusion. Incidentally, the  
reaction portion 1 and the solution storage portion 2  
are separately prepared, and the solution storage  
portion 2 may be superimposed on the reaction portion  
1 at the time of use.

20 ~~To the side surface of the biochemical reaction~~  
~~cartridge, a~~ A bar code label 40 for identifying the  
type of cartridge is adhered to the side surface of  
the biochemical reaction cartridge. When the  
biochemical reaction cartridge is set to a treatment  
25 apparatus described later, the bar code is read and  
the type of the cartridge is identified from the  
result. Setting of the treatment apparatus is



automatically performed, so as to effect an appropriate treatment procedure.

Figure 2 is a plan view of the solution storage portion 2 of Figure 1. Referring to Figure 2, the solution storage portion 2 is provided with independent chambers 6a to 6m, each containing a solution. In the chambers 6 and 6b, a first hemolytic agent containing EDTA (ethylenediaminetetraacetic acid) for destructing cell wall and a second hemolytic agent containing a ~~protein~~-protein-modifying agent, such as a surfactant, are stored, respectively.

In the chamber 6c, particles of magnetic material coated with silica, by which DNA is adsorbed, are stored. In the chambers 6l and 6m, a first extraction cleaning liquid and a second extraction cleaning liquid, which are used for purifying DNA at the time of extraction of DNA, are stored, respectively.

An eluent, comprising a buffer of low concentration salt, for eluting DNA from the magnetic particles, is stored in the chamber 6d, ~~a.~~ A mixture liquid for PCR (~~polymeraze~~-polymerase chain reaction) comprising a primer, polymerase, a dNTP (deoxyribonucleotide triphosphate), a buffer, Cy-3dUTP containing a fluorescent agent, etc., is stored in the chamber 6g. In the chambers 6h and 6j, a cleaning agent containing a surfactant for cleaning a fluorescence-labeled specimen DNA, which is not

subjected to hybridization, and a fluorescence label  
are stored. In the chamber 6i, alcohol for drying the  
inside of a chamber including a DNA microarray, which  
is described laterbelow, is stored. The respective  
5 chambers 6a to 6m are provided with a sharp-pointed  
valve stems (rods) 7a to 7m, respectively, described  
laterbelow, for penetrating the sheets.

Figure 3 is a sectional view showing a storage  
state in the biochemical reaction cartridge.  
10 Referring to Figure 3, the valve stem 7 provided with  
a cut 8 is injected into the chamber 6, ~~containing a~~  
~~solution,~~ of the solution storage portion 2, which  
contains a solution, ~~the valve stem 7 provided with a~~  
~~cut 8 is injected and~~ is supported by two o-rings.  
15 The bottom of the solution chamber 6 is blocked by an  
aluminum foil sheet 10. A sealing member 12 is  
disposed between the chamber 6 and the chamber 11 of  
the reaction portion 1, so as to make it impossible  
for air to enter and exit. Changes in volume of the  
20 solution and air and in pressure due to the  
environment can be ~~adsorbed~~ accommodated by the  
deformation of the aluminum foil sheet 10, so that the  
solution in the chamber 6 cannot unexpectedly enter  
the reaction portion 1.

25 Figure 4 illustrates ~~such a state that in which~~,  
after a tester injects a liquid specimen, such as  
blood, from the specimen port 3 and sets the

biochemical reaction cartridge to a treatment  
apparatus described ~~later~~below, a robot arm (not  
shown) presses the valve stem 7 by first-stage pushing  
with a shorter pressing rod 13a of a rod needle 13 to  
5 ~~stare~~tear the aluminum foil sheet, thus starting the  
movement of the solution from the chamber 6 to the  
chamber 11. In this state, the two O-rings 8 are  
located in the cut 8 of the valve stem 7, so that the  
chamber 6 communicates with outside air. Accordingly,  
10 the solution can be moved smoothly.

As described above, the biochemical reaction  
cartridge has the penetrable aluminum sheet 10 as a  
partition member, so that only by ~~the~~-pressing the  
pressing rod 13a of the tool needle 13 toward the  
15 reaction portion 1, it is possible to readily cause  
the solution to flow from the chamber 6 into the  
chamber 11 without ~~causing contact of the tool needle~~  
13 coming into contact with the solution.  
Incidentally, in this embodiment, immediately under  
20 the position of the chamber of the solution storage  
portion 2, a corresponding chamber of the reaction  
portion 1 is located, but there is no harm in shifting  
the corresponding chamber from the position  
immediately under the chamber of the solution storage  
25 portion 2 if, e.g., a passage is provided  
therebetween.

In this embodiment, the chamber of the reaction

portion 1 and the chamber of the solution storage  
portion 2 are in a one-to-one relationship, but a  
plurality of solution storage chambers may be provided  
per one chamber for the reaction portion 1. Further,  
5 in this embodiment, the solution is moved from the  
solution storage chamber to a blank chamber of the  
reaction portion 1, but it may be moved from the  
solution storage chamber to a chamber of the reaction  
portion 1 already containing a specimen or a solution  
10 during treatment. Further, in this embodiment, the  
aluminum foil sheet 10 is used as the partition  
member, but the partition member per se may be a  
non-penetrable member if it is provided with an  
ordinary valve, and the valve is placed in a  
15 penetrable state, i.e., an open state so as to permit  
the flowing of the solution into the chamber of the  
reaction portion 1.

Next, the tester ~~once~~ extracts the tool needle 13  
from the treatment apparatus once by using the robot  
20 arm and turns the tool needle 13 upside down, followed  
by further pressing the valve stem 7 by second-stage  
pushing with a longer pressing rod 13b, as shown in  
Figure 5. As a result, air is sealed up by the upper  
O-ring 9 to permit the movement of the solution in the  
25 reaction portion 9 to permit the movement of the  
solution in the reaction portion 1, as described  
~~later~~below. The tester performs this step with

respect to all the chambers 6a to 6m. As described above, the solution can be caused to flow into the chamber by the first-stage pushing, and the chamber can be sealed up by the second-stage pushing, so that  
5 it is possible to effect the ~~flowing~~ of the solution into the chamber 11 and ~~sealing off~~ the chamber 11 at the same time only by simple pushing operations. Further, the above-described tool needle may be provided in the biochemical reaction cartridge.

10 Figure 6 is a plan view of the reaction portion 1. Referring to Figure 6, ~~on one side surface of the reaction portion 1~~, 10 nozzle ports 4a to 4j are provided on one side surface of the reaction portion ~~and also on the other side surface thereof~~.  
15 nozzle ports 4k to 4t are provided. The respective nozzle ports 4a to 4t communicate with chambers 11a to 11t, which are portions or sites for storing the solution or causing a reaction, through corresponding air passages 14a to 14t for air flow, respectively.

20 In this embodiment, however, the nozzle ports 4n, 4p, 4q and 4s are not used, ~~to~~. These nozzle ports do not communicate with the chambers and are used as reserve ports. More specifically, in this embodiment, the nozzle ports 4a to 4j communicate with the  
25 chambers 11a to 11j through the passages 14a to 14j, respectively. On the other side surface, the nozzle ports 4k, 4l, 4m, 4o, 4r and 4t communicate with the

chambers 11k, 11l, 11m, 11o, 11r and 11t through the passages 14k, 14l, 14m, 14o, 14r and 14t, respectively.

The specimen port 3 communicates with a chamber  
5 16. The chambers 11a, 11b, 11c and 11k communicate with the chamber 16, the chambers 11g and 11o communicate with a chamber 17, and the chambers 11h, 11i, 11j, 11r and 11t communicate with a chamber 18. Further, the chamber 16 communicate with the chamber  
10 17 via a passage 19, and the chamber 17 communicates with the chamber 18 via a passage 20. With the passage 19, the chambers 11d, 11e, 11f, 11l and 11m communicate via passages 15d, 15e, 15f, 15l and 15m, respectively. At a bottom (undersurface) of the  
15 chamber 18, a square hole is provided. ~~To the square hole, a~~ A DNA microarray 21, on which several tens to several hundreds of thousand of different species of DNA probes are arranged ~~in~~ at high density on a surface of a solid phase, such as a glass plate having  
20 a size of ca. one square centimeter, with the probe surfaces up, is attached to the square hole.

It is possible to test a large number of genes at the same time by ~~effecting a hybridization reactioning~~ with the specimen DNA ~~with the use of~~ using the  
25 microarray 21.

The DNA probes are regularly arranged in a matrix form, and an address (position determined by

the row and column numbers ~~of row and the number of~~  
~~column~~ on the matrix) of each of the DNA probes is  
readily read as information. The genes to be tested  
includes, e.g., genetic polymorphism of each  
5 individual in addition to infections viruses, bacteria  
and disease-associated genes.

In the chambers 11a and 11b of the reaction  
portion 1, a first hemolytic agent and a second  
hemolytic agent to be moved from the chambers 6a and  
10 ~~6b~~7 and the solution storage portion 2 are stored,  
respectively. In the chamber 11c, magnetic material  
~~particles of magnetic material~~ to be moved from the  
chamber 6 are stored. In the chambers 11l and 11m, a  
first extraction cleaning liquid and a second  
15 extraction cleaning liquid to be moved from the  
chambers 6l and 6m are stored, respectively. An  
eluent flowing from the chamber 6d is stored in the  
chamber 11d, a mixture liquid necessary for PCR  
(~~polymerase~~polymerase chain reaction) moved from the  
20 chamber 6g is stored in the chamber 11g. In the  
chambers 11h and 11j, cleaning agents to be moved from  
the chambers 6h and 6j are stored, respectively. In  
the chamber 11i, alcohol to be moved from the chamber  
6i is stored.

25 The chamber 11e is a chamber in which dust<sub>1</sub> other  
than DNA ~~of~~from blood<sub>1</sub> accumulates, the chamber 11f  
is a chamber in which waste of the first and second

extraction cleaning liquids in the chambers 11l and  
11m accumulates, the chamber 11r is a chamber in which  
waste of the first and second cleaning agents  
accumulates, and the chambers 11k, 11o and 11t are  
5 blank chambers provided for preventing the solution to  
from flowing into the nozzle ports.

Figure 7 is a schematic view of the treatment  
apparatus for controlling the movement of the solution  
within the biochemical reaction cartridge and various  
10 reactions.

~~On a table 22, the~~ The biochemical reaction  
cartridge is mounted on a table 22. Further, ~~on the~~  
~~table 22,~~ an electromagnet 23 to be actuated at the  
time of extracting DNA or the like from the specimen  
15 in the cartridge 1, a Peltier element 24 for effecting  
temperature control at the time of amplifying DNA from  
the specimen through a method such as PCR (polymerase  
chain reaction), and a Peltier element 25 for  
effecting temperature control at the time of  
20 performing a hybridization between the amplified  
specimen DNA and the DNA probe on the DNA microarray  
within the cartridge 1 and at the time of cleaning or  
washing the specimen DNA, which is not hybridized, are  
disposed on the table 22 and connected to a control  
25 unit 26 for controlling the entire treatment  
apparatus. Further, the robot arm (not shown) for  
pushing down the valve stem by moving the tool needle



13 above a predetermined chamber on the cartridge, as  
described above, and a bar code reader (not shown) for  
reading the bar code label applied to the cartridge  
are provided ~~to~~ in the treatment apparatus.

5       At both side surfaces of the table 22, an  
electric (motor-driven) syringe pumps 27 and 28 and  
pump blocks 31 and 32, each of which is a port for  
discharging or sucking in air by these pumps 27 and 28  
and is provided with 10 pump nozzles 29 or 30 on its  
10 side surface, are disposed. Between the electric  
syringe pumps 27 and 28 and the pump nozzles 29 and  
30, a plurality of known electric switching (selector)  
valves (not shown) are disposed and connected to the  
control unit 26 together with the pumps 27 and 28.  
15 The control unit 26 is connected to an input unit 33  
to which inputting by a tester is performed. The  
control unit 26 controls the pump nozzles 29 and 30,  
so that each of the respective 10 pump nozzles is  
selectively opened and closed with respect to the  
20 electric syringe pumps 27 and 28, respectively.

When the solution is moved from the solution  
storage portion 2 to the reaction portion 1 and a  
treatment start signal is inputted, extraction and  
amplification of DNA or the like are performed within  
25 the reaction portion 1. Further, hybridization  
between the amplified specimen DNA and DNA probes on  
the DNA microarray disposed in the reaction portion 1

and cleaning of the fluorescence-labeled specimen DNA, which is not hybridized, and the fluorescence label are performed.

In this embodiment, when the tester injects blood  
5 as a specimen into the reaction portion through the rubber cap of the specimen port 3 by a syringe or an injector, the blood flows into the chamber 16. Thereafter, the tester places the biochemical reaction cartridge on the table 22 and moves the pump blocks 31  
10 and 32 in directions indicated ~~of~~ by the arrows ~~indicated~~ in Figure 7 with a mechanism (not shown) by operating ~~an unshown~~ a lever (not shown), whereby the pump nozzles 29 and 30 are injected into the corresponding nozzle ports 4 of the reaction portion  
15 1.

As described with reference to Figure 6, the nozzle ports 4 are concentrated at two surfaces, i.e., both side surfaces, of the biochemical reaction cartridge, so that it is possible to simplify shapes  
20 and arrangements of the electric syringe pumps 27 and 28, the electric switching valves, the pump blocks 31 and 32 containing the pump nozzles 29 and 30, etc. Further, by effecting such a simple operation that the cartridge is sandwiched between the pump blocks 31 and  
25 32 at the same time while ensuring necessary chambers and passages, it is possible to inject the pump nozzles 29 and 30 and simplify the structure of the

pump blocks 31 and 32. Further, all the nozzle ports 4a to 4t are disposed at an identical level, i.e., are arranged linearly, whereby all the heights of the passages 14a to 14t connected to the nozzle ports 4a to 4t become equal to each other. As a result, preparation of the passages 14a to 14t becomes easy.

Further, in the treatment apparatus shown in Figure 7, in the case where the length of the pump blocks 31 and 32 is increased n times the original length with respect to n biochemical reaction cartridges, when ~~the n~~ cartridges are arranged in series, it is possible to perform a necessary step with respect to all the n cartridges at the same time. As a result, a biochemical reaction can be performed in ~~the a~~ a large number of biochemical reaction cartridges with a very simple apparatus structure.

When the tester performs the steps of flowing of the solution into the chamber and hermetically sealing the chamber described with reference to Figures 4 and 5 and then inputs a treatment start instruction at the input unit 33, the bar code label applied to the biochemical reaction cartridge is first read by the bar code reader (not shown) of the treatment apparatus. In the treatment apparatus, treatment sequences necessary for the respective types of cartridges are memorized in advance. When the type of cartridge is identified by the read bar code, the

contents and procedures of treatment necessary for the cartridge are automatically determined to start the treatment. When the bar code cannot be read or the read bar code is not a predetermined bar code, the  
5 tester can also manually input treatment steps by the input unit 33.

~~Figure 8 (consisting of Figures 8A and 8B) is~~  
show a flow chart for explaining an example of a treatment procedure in the treatment apparatus in this  
10 embodiment.

Referring to Figure 8A, in ~~a~~-step S1, the first hemolytic agent is moved from the solution storage chamber 6a to the chamber 11a of the reaction portion 1 by ~~effecting injection of~~injecting the solution and  
15 hermetic sealing, as described with reference to Figures 4 and 5. In ~~a~~-step S2, the control unit 26 opens only the nozzle ports 4a and 4b, and air is discharged from the electric syringe pump 27 and sucked in the reaction portion 1 from the electric  
20 syringe pump 28, whereby the first hemolytic agent is injected from the chamber 11a into the chamber 16 containing blood. At this time, by controlling air suction ~~of air~~ from the pump 28 so as to start 10 - 200 msec after initiation of the air discharge from  
25 the pump 27, the solution can flow smoothly without causing splashing or scattering ~~thereof~~ at its leading end, although it ~~this~~ depends on ~~a~~ the viscosity of

the hemolytic agent and a resistance of the passage.

As described above, by shifting the timing of the supply and suction of air so as to control a manner ~~of~~ in which the pressure is application-applied and  
5 ~~pressure reduction~~reduced, it is possible to cause the solution to flow smoothly. In a preferred embodiment, the solution can be caused to flow ~~further~~even more smoothly by effecting ~~such a controlling that a degree of~~air suction ~~of air~~ from the electric syringe pump 28  
10 such that it is linearly increased from the initiation of the air discharge from the pump 27. Further, it becomes possible to alleviate the pressure generated in the reaction portion 1 by applying and reducing pressure in combination. As a result, it is also  
15 possible to ~~achieve such an effect that the solution is prevented intentionally prevent the solution from~~ flowing into a branched passage or chamber ~~in the case during the movement thereof where the solution is not intended to flow into the branched passage or chamber~~  
20 ~~curing movement thereof. These are~~This is also true in the case of a subsequent liquid movement.

The air supply control can be readily realized by using the electric syringe pumps 27 and 28. More specifically, after only the nozzle ports 4a and 4o  
25 are opened, discharge and suction of air are repeated alternately by the syringe pumps 27 and 28 to cause a repetitive flow and ~~flowback~~return of the solution of

the chamber 6 in the passage 19, thus stirring the solution. Alternatively, the solution can be stirred while continuously discharging air from the pump 28 to generate bubbles.

5           Figure 9 is a sectional view of the reaction portion 1 shown in Figure 6 along a ~~eress~~cross-section intersecting the chambers 11a, 16 and 11k, and shows such a state that the nozzle port 4a is pressurized by injecting therein the pump nozzle 29  
10 and the nozzle port 4k is reduced in pressure by injecting therein the pump nozzle 30, whereby the first hemolytic agent in the chamber 11a flows into the chamber 16 containing blood.

Referring again to Figure 8A, in ~~a~~-step S4, only  
15 the nozzle ports 4b and 4k are opened and the second hemolytic agent in the chamber 11b is caused to flow into the chamber 16 in the same manner as in the case of the first hemolytic agent. Similarly, in ~~a~~-step S5, the magnetic particles in the chamber 11, after  
20 being moved from the chamber 6c to the chamber 11, are caused to flow into the chamber 16. In ~~the~~-steps S4 and S6, stirring is performed in the same manner as in ~~the~~-step S2. In ~~the~~-step S6, DNA resulting from dissolution of cells in ~~the~~-steps S2 and S4 attaches  
25 to the magnetic particles.

Thereafter, in ~~a~~-step S7, an electromagnet 23 is turned on and only the nozzle ports 4e and 4k are

opened. Then, air is discharged from the electric syringe pump 28 and sucked in from the pump 27 to move the solution from the chamber 16 to the chamber 11e. At the time of movement, the magnetic particles and DNA are trapped in the passage 19 on the electromagnet 23. The suction and discharge by the pumps 27 and 28 are alternately repeated to reciprocate the solution two times between the chambers 16 and 11e, whereby a trapping efficiency of DNA is improved. The trapping efficiency can be further improved by increasing the number of reciprocations. In this case, however, ~~it takes a longer treating time by that much~~ the time of treatment is increased by the amount of time it takes to perform the additional reciprocations.

As described above, DNA is trapped in a flowing state on such a small passage having a width of about 1 - 2 mm and a height of about 0.2 - 1 mm by utilizing the magnetic particles, so that DNA can be trapped with a high efficiency. This is also true for RNA and proteins.

Then, in ~~a~~-step S8, the electromagnet 23 is turned off, and only the nozzle ports 4f and 4l are opened. Thereafter, air is discharged from the electric syringe pump 28 and sucked in from the pump 27 to move the first extraction cleaning liquid from the chamber 11l to the chamber 11f. At this time, the magnetic particles and DNA trapped in ~~the~~-step S7 are

moved together with the extraction cleaning liquid,  
whereby cleaning is performed. After the  
reciprocation ~~of~~ is performed two times ~~is performed~~  
in the same manner as in ~~the~~ step S7, the  
5 electromagnet 23 is turned on, and the reciprocation  
~~of~~ is similarly performed two times ~~is similarly~~  
~~performed~~ to recover the magnetic particles and DNA in  
the passage 19 on the electromagnet 23 and return the  
solution to the chamber 11l.

10 In ~~a~~ step S11, cleaning is further performed in  
the same manner as in ~~the~~ step S5 by using the second  
extraction cleaning liquid in the chamber 11m, after  
being moved from the chamber 6m to the chamber 11m in  
~~a~~ step S10, in combination with the nozzle ports 4f  
15 and 4m.

In ~~a~~ step 12, the eluent is moved from the  
chamber 6d to the chamber 11d. In ~~a~~ step S13, only  
the nozzle ports 4d and 4o are opened while the  
electromagnet 23 is kept on, and air is discharged  
20 from the pump 27 and sucked in from the pump 28,  
whereby the eluent in the chamber 11d is moved to the  
chamber 17.

At this time, the magnetic particles and DNA are  
separated by the action of the eluent, so that  
25 only the DNA is moved together with the eluent to the  
chamber 17, and the magnetic particles remain in the  
passage 19. Thus, extraction and purification of the



DNA are performed. As described above, the chambers 11l and 11m containing the extraction cleaning liquids and the chamber 11f containing a waste liquid after the cleaning are separately provided, so that it  
5 becomes possible to effect extraction and purification of the DNA in the biochemical reaction cartridge.

Next, in ~~a~~-step S14, the PCR agent is moved from the chamber 6g to the chamber 11g. In ~~a~~-step S15, only the nozzle ports 4g and 4o are opened, and air is  
10 discharged from the electric syringe pump 27 and sucked in from the pump 28 to cause the PCR agent in the chamber 11g to flow into the chamber 17. Further, only the nozzle ports 4g and 4t are opened~~7~~ and air discharge and suction by the pumps 27 and 28 are  
15 repeated alternately to cause the solution in the chamber 16 to flow into the passage 20. Thereafter, the returning operation is repeated to effect stirring. Then, the Peltier element 24 is controlled to retain the solution in the chamber 17 at 96 °C for  
20 10 min. Thereafter, a cycle of heating at 96 °C/10 sec, 55 °C/10 sec, and 72 °C/1 min. is repeated 30 times, thus subjecting the eluted DNA to PCR to amplify the DNA.

In ~~a~~-step S16, only the nozzle ports 4g and 4t  
25 are opened~~7~~ and air is discharged from the electric syringe pump 27 and sucked in from the pump 28 to move the solution in the chamber 17 to the chamber 18.

Further, by controlling the Peltier element 25, the solution in the chamber 18 is kept at 45 °C for 2 hours to effect the hybridization. At this time, discharge and suction of air by the pumps 27 and 28  
5 are repeated alternately to move the solution in the chamber 18 to the passage 15t. Thereafter, the hybridization proceeds while effecting stirring by repeating the returning operation.

Then, after the first cleaning liquid is moved  
10 from the chamber 6h to the chamber 11h in a step S17, in a step S18, while keeping the temperature at 45 °C, only the nozzle ports 4h and 4r are opened, and air is discharged from the electric syringe pump 27 and sucked in from the pump 28 to cause the first cleaning  
15 liquid in the chamber 11h to flow into the chamber 11r through the chamber 18 while moving the solution in the chamber 18 to the chamber 11r. The suction and discharge by the pumps 27 and 28 are repeated alternately to reciprocate the solution two times  
20 between the chambers 11h, 18 and 11r and finally return the solution to the chamber 11h. Thus, the fluorescence-labeled specimen DNA and the fluorescence label, which are not hybridized, are cleaned.

Figure 10 is a sectional view of the reaction  
25 portion 1 shown in Figure 6 along a ~~eross~~cross-section intersecting the chambers 11h, 18 and 11r. The reaction portion 1 is pressurized by injecting the

pump nozzle 29 into the nozzle port 4h and ~~is reduced~~  
~~in the~~ pressure is reduced by injecting the pump nozzle  
30 into the nozzle port 4r. Figure 10 illustrates  
such a state that the first cleaning liquid is caused  
5 to flow into the chamber 11r through the chamber 18.  
The chamber 11h actually communicates with the  
solution storage portion 2, but in Figure 10, it is  
illustrated as a ~~state in which it does not~~  
~~communicate~~ communicating with the solution storage  
10 portion 2 by providing a ceiling thereof, for the  
convenience of ~~explanation~~ explaining the structure.

Referring ~~again~~ to Figure 8B, after the second  
cleaning liquid is moved from the chamber 6j to the  
chamber 11j in a ~~step~~ S19, in a ~~step~~ S20, while  
15 keeping the temperature at 45 °C, the cleaning is  
further effected in the same manner as in ~~the~~ step S10  
by using the second cleaning liquid in the chamber 11j  
in combination with the nozzle ports 4j and 4r, and  
the solution is finally returned to the chamber 11j.  
20 As described above, the chambers 11h and 11j  
containing the cleaning liquids and the chamber 11r  
containing the waste liquid after the cleaning are  
separately provided, so that it becomes possible to  
~~effect extraction and purification~~ purify of the  
25 biological material on the DNA microarray 21 in the  
biochemical reaction cartridge.

After alcohol is moved from the chamber 6i to the

chamber 11i in a—step S21, in a—step 22, only the  
nozzle ports 4i and 4r are opened~~7~~ and air is  
discharged from the electric syringe pump 27 and  
sucked in from the pump 28 to move alcohol in the  
5 chamber 11i to the chamber 11r through the chamber 18.  
Thereafter, only the nozzle port 4i and 4t are opened~~7~~  
and air is discharged from the pump 27 and sucked in  
from the pump 28 to dry the inside of chamber 18.

Thereafter, when the tester operates a lever (not  
10 shown), the pump blocks 31 and 32 are moved away from  
the biochemical reaction cartridge. As a result, the  
pump nozzles 29 and 30 are removed from the nozzle  
ports 4 of the cartridge. Then, the tester mounts the  
cartridge in a DNA microarray reader~~for DNA~~  
15 ~~microarray~~, such a known scanner~~,~~ to ~~effect~~perform  
the measurement and analysis.

In the above-described embodiment, the  
identification of the cartridge is performed by using  
the bar code label~~,~~ but may also be performed by using  
20 a two-dimensional bar code, an IC chip, PFID (radio  
frequency identification), etc. Further, on the basis  
of external dimensions of the cartridge~~,~~ such as  
height and length, the number of recesses or  
projections provided on the side surfaces, the upper  
25 surface and the lower surface of the cartridge, and a  
combination thereof, the type of the cartridge can be  
identified in various ~~manner~~sways. As a result, it is

possible to attain a similar effect.

In the above embodiment, the identification of the cartridge is performed and based on the identified type of the cartridge, and the treatment steps are  
5 set. However, it is also possible to set a treatment sequence on the basis of the information, ~~on the~~ contents and procedures of the treatment steps, which are written in the two-dimensional bar code or the like. Further, in the case of changing testing  
10 conditions, such as a reaction time, cartridge by cartridge, different treatment steps are written in a two-dimensional bar code and the bar code is adhered to the cartridge, whereby it becomes possible to effect a desired reaction step with reliability.

15 As described ~~hereinabove~~, the biochemical reaction cartridge according to the present invention has a reaction portion including a chamber and a passage and a solution storage portion, which is isolated or separated from the reaction portion, for  
20 storing a solution, such as a reagent or a cleaning agent, and is constituted by such a member that it is separated for moving the solution from the solution storage portion to the reaction portion and is penetrable, or that it is a penetrable member disposed  
25 at a boundary wall portion between the solution storage portion and the reaction portion, which contact each other. As a result, respective solutions

can be prepared with the biochemical reaction cartridge immediately before the respective treatment steps, so that the biochemical reaction cartridge has the advantage of causing an intended reaction properly  
5 without causing a reagent in a chamber to flow into a passage or another chamber even when an environmental change or vibration occurs during a treatment step using another solution.

Further, particularly, a step of moving each of  
10 the solutions in the solution storage portion to the reaction portion immediately before use-ing the solutions is employed, so that it is possible to reliably effect ~~reliable-the~~ reaction without causing the solutions to flow into adjacent chambers and  
15 passages even when ~~vibration-of~~ the treatment apparatus ~~occurs-vibrates~~ or there ~~arises-is~~ an error ~~of-in~~ pressure control during treatment in each of the steps.

Further, the treatment apparatus automatically  
20 reads the bar code label applied to the biochemical reaction cartridge and identifies the type of the cartridge, thus automatically setting necessary treatment steps. Accordingly, it becomes possible to simply effect the treatment with reliability since it  
25 is not necessary for the operation to set a complicated treatment procedure on all such occasions that there ~~are-is~~ a plurality of cartridge types.

Further, since the biochemical reaction cartridge of the present invention has the above-described structure, it is possible to prepare a solution therein as desired. As a result, the biochemical  
5 reaction cartridge eliminates the inconvenience of replenishing a reagent and reduces an error in selection of the type of reagent. In addition, even when an environmental change or vibration ~~is caused to~~ occurs at the time of storage and conveyance, the  
10 reagent in the chamber does not flow into a passage or another chamber. Accordingly, the biochemical reaction cartridge can appropriately cause ~~an~~ the intended reaction ~~appropriately~~.

While the invention has been described with  
15 reference to the structures disclosed herein, it is not ~~confined~~ limited to the details set forth and this application is intended to cover such modifications or changes as may come within the purposes of the improvements or the scope of the following claims.

ABSTRACT OF THE DISCLOSURE

A biochemical reaction cartridge includes a reaction portion, comprising a chamber and a passage,  
5 for effecting a biochemical reaction, and a solution storage portion, which is isolated or separated from said reaction portion, for storing a solution in a position corresponding to the chamber. The cartridge is provided with a penetrable partition member  
10 disposed between ~~said~~the solution storage portion and ~~said~~the reaction portion, so as to move the solution from ~~said~~the solution storage portion to the chamber of ~~said~~the reaction portion. The biochemical reaction cartridge is incorporated in a biochemical  
15 reaction apparatus.